Three-dimensional quantitative ultrasound for detecting lymph node metastases

Emi Saegusa-Beecroft, MD,a,b,* Junji Machi, MD, PhD, FACS,a Jonathan Mamou, PhD,c Masaki Hata, MD, PhD,d Alain Coron, PhD,e,f Eugene T. Yanagihara, MD, FCAP,b Tadashi Yamaguchi, PhD,g Michael L. Oelze, PhD,h Pascal Laugier, PhD,e,f and Ernest J. Feleppa, PhD, FAIUM, FAIMBEc

aDepartment of Surgery, University of Hawaii and Kuakini Medical Center, Honolulu, Hawaii
bDepartment of Pathology, Kuakini Medical Center, Honolulu, Hawaii
cLizzi Center for Biomedical Engineering, Riverside Research, New York, New York
dDepartment of Surgery, Juntendo University, School of Medicine, Tokyo, Japan
eUniversity Pierre and Marie Curie, Université Paris 06, Paris, France
fCentre National de la Recherche Scientifique, Laboratoire d’Imagerie Paramétrique, Paris, France
gResearch Center for Frontier Medical Engineering, Chiba University, Chiba, Japan
hDepartment of Electrical and Computer Engineering, University of Illinois, Urbana, Illinois

Abstract

Purpose: Detection of metastases in lymph nodes (LNs) is critical for cancer management. Conventional histological methods may miss metastatic foci. To date, no practical means of evaluating the entire LN volume exists. The aim of this study was to develop fast, reliable, operator-independent, high-frequency, quantitative ultrasound (QUS) methods for evaluating LNs over their entire volume to effectively detect LN metastases.

Methods: We scanned freshly excised LNs at 26 MHz and digitally acquired echo-signal data over the entire three-dimensional (3D) volume. A total of 146 LNs of colorectal, 26 LNs of gastric, and 118 LNs of breast cancer patients were enrolled. We step-sectioned LNs at 50-μm intervals and later compared them with 13 QUS estimates associated with tissue microstructure. Linear-discriminant analysis classified LNs as metastatic or nonmetastatic, and we computed areas (Az) under receiver-operator characteristic curves to assess classification performance. The QUS estimates and cancer probability values derived from discriminant analysis were depicted in 3D images for comparison with 3D histology.

Results: Of 146 LNs of colorectal cancer patients, 23 were metastatic; Az = 0.952 ± 0.021 (95% confidence interval [CI]: 0.911–0.993); sensitivity = 91.3% (specificity = 87.0%); and sensitivity = 100% (specificity = 67.5%). Of 26 LNs of gastric cancer patients, five were metastatic; Az = 0.962 ± 0.039 (95% CI: 0.807–1.000); sensitivity = 100% (specificity = 95.3%). A total of 17 of 118 LNs of breast cancer patients were metastatic; Az = 0.833 ± 0.047 (95% CI: 0.741–0.926); sensitivity = 88.2% (specificity = 62.5%); sensitivity = 100% (specificity = 50.5%). 3D cancer probability images showed good correlation with 3D histology.

Conclusions: These results suggest that operator- and system-independent QUS methods allow reliable entire-volume LN evaluation for detecting metastases. 3D cancer probability images showed good correlation with 3D histology.
images can help pathologists identify metastatic foci that could be missed using conventional methods.

1. Introduction

For many cancers, accurate detection of metastases in lymph nodes (LNs) is crucial to determine the disease stage using the American Joint Committee on Cancer tumor-node-metastases staging system. Changes in the node status affect treatment and management. The latest edition categorizes micrometastases (0.2–2 mm) and isolated tumor cells (<0.2 mm or <1000 tumor cells) separately from macrometastases. Micrometastases are considered to be clinically significant and positive for metastases [1].

For all cancers, pathologists currently perform a microscopic histologic examination of surgically dissected LNs. For colorectal cancer and gastric cancer, only one central histological section of each LN is usually evaluated for metastases, regardless of LN size [2,3]. For invasive carcinoma of the breast, the College of American Pathologists recommends that each LN should be sliced parallel to the long axis of the LN at a spacing of 2 mm. These slices are then submitted for microscopic examination with at least one representative hematoxylin and eosin (H&E)—stained thin section obtained from the surface of each slice examined histologically [4].

To date, no method is clinically available for examining LNs in their entire volume to detect metastases. Molecular studies such as reverse transcription polymerase chain reaction have been reported [5–8], but continue to be a research topic and have not been adopted for clinical practice. There is some consensus in the literature that treatment decisions should not yet be based on these techniques [1–4,9–12]. The reference standard remains histologic examination of H&E histology, and occasionally additional sections from the specimen may be required for subsequent special staining, such as immunohistochemical methods [4,13,14]. With the conventional method, unless the metastases are included in the section examined microscopically, metastases, particularly micrometastases, may be missed [15–22].

Breast sentinel LN biopsy now is well established in the United States for clinically node-negative axillae [9,23]. Touch-prep imprinting and frozen-section procedures for detection of metastases provide limited sensitivity because of sampling limitations [9,24–28]. Multiple-level step sectioning of specimens has been reported to detect more metastases [15–18,20–22]. Different countries and facilities have reported their own protocols for multilevel step-sectioning at different intervals of axillary sentinel LNs of breast cancer patients [4,29–31], but to date, no international consensus on an optimal histopathology procedure exists [31]. The clinical impact on the outcome of detecting occult micrometastases and isolated tumor cells remains controversial [4,17,21,32–35]. Recently, the need to complete a formal axillary LN dissection in patients with a positive sentinel LN biopsy showing macrometastases or micrometastases in fewer than three nodes has been questioned [36] and remains controversial [37]. However, many of these studies do not account for the potential true residual disease prevalence in axillary LNs, because metastases are detected using limited conventional histopathologic procedures. If a new method could be developed to rapidly assess LNs for suspicion of metastases non-invasively over the entire LN volume before histology processing, the new method would resolve the current controversies and would have broad implications for staging a wide range of cancers.

The aim of our study was to develop a fast, reliable, and operator-independent method for entire-volume LN examination to detect and image LN metastases using high-frequency (HF) quantitative ultrasound (QUS) [38,39]. By using HF ultrasound (i.e., >15 MHz) and digitally acquiring and analyzing the ultrasound echo signals, QUS methods can provide estimates of tissue microstructure on a subresolution scale. Unlike B-mode ultrasound images currently used clinically, QUS methods are operator independent and provide a quantitative means of estimating microscopic-scale tissue properties. These attributes, combined with the ability of three-dimensional (3D) ultrasound scans to acquire data from the full LN volume, enable QUS methods to evaluate the entire LN and detect micrometastases as well as macrometastases. Future clinical 3D QUS systems potentially will enable surgeons and pathologists to detect metastatic LNs with high sensitivity.

2. Materials and methods

2.1. Enrollment

A total of 160 patients (44 men and 116 women) with histologically proven colorectal, gastric, and breast cancer, who underwent cancer surgery at the Kuakini Medical Center in Honolulu, Hawaii, were randomly and consecutively enrolled in this prospective study. This patient cohort included 71 patients (all women) with breast cancer, 77 patients (38 men and 39 women) with colorectal cancer, and 12 patients with gastric cancer (6 men and 6 women). The median age for each cancer type was: breast, 65 y (range, 42–93 y; mean, 67.4 y; standard deviation [SD], 12.5 y); colorectal, 74 y (range, 40–95 y; mean, 71 y; SD, 13.1 y); and gastric, 81.5 y (range, 52–93 y; mean, 76.3 y; SD, 14.1 y).

Institutional review boards at the University of Hawaii and the Kuakini Medical Center approved the study protocol. We obtained written informed consent from all patients.

2.2. Materials

Study materials were LNs harvested from surgical specimens dissected from previously untreated patients with histologically proven colorectal, gastric, or breast cancer; axillary sentinel LNs that underwent an imprint (i.e., “touch-prep”) cytology procedure satisfied this criterion. The study excluded
LNs with undetermined primary cancer origins, LNs undergoing a frozen-section procedure because of potential tissue damage, large LNs that did not fit in the standard embedding cassette (3.0 × 2.6 cm), and LNs that were retrieved after formalin fixation or immersion in fat-clearing solutions. We harvested LNs from freshly excised gross surgical specimens submitted to pathology for standard of care histologic evaluation. We carefully removed excess perinodal adipose tissue during the LN harvest, leaving 0.3–0.5 mm of surrounding fat layer to avoid inadvertently removing lymphoid tissue. The study procedures did not interfere with the standard of care pathology protocol, but added histologic information by microscopically examining each LN over its entire volume by step-sectioning, instead of using conventional methods, which only examine thin sections obtained from the central plane of the node or from 2-mm-thick sections.

The investigator was independent of the surgical and the pathology service and did not have access to clinical information. The investigator performing the dissections was informed only that the LNs were dissected from histologically proven colorectal, and gastric, and breast cancer patients, and was blinded from clinical information such as clinical presentation, history, physical examination, palpable LN status, primary tumor properties such as histologic type, size, grade, and so forth. Freshly excised LNs were randomly selected from the gross surgical specimen and were immediately submerged in 0.9% normal saline, pinned to a sound-absorbing material, and then scanned with HF ultrasound to acquire radiofrequency (RF) echo-signal data.

### 2.3. High-frequency ultrasonic data acquisition

We designed a custom, HF ultrasound, laboratory scanning system and built it to acquire RF echo-signal data in 3D from

---

**Table:** Classification performance

<table>
<thead>
<tr>
<th>Cancer type</th>
<th>Effective QUS estimates</th>
<th>55% Confidence interval</th>
<th>Area under ROC curve</th>
<th>95% Confidence interval</th>
<th>Sensitivity</th>
<th>Specificity</th>
</tr>
</thead>
<tbody>
<tr>
<td>Colorectal</td>
<td>Scatter size, Nakagami a, quartile-quantile Sa</td>
<td>0.991–0.993</td>
<td>0.992 ± 0.021</td>
<td>0.922 ± 0.039</td>
<td>0.920–1.000</td>
<td>0.807–1.000</td>
</tr>
<tr>
<td>Gastric</td>
<td>Scatter size, intercept, quartile-quantile Cy</td>
<td>0.993–0.996</td>
<td>0.992 ± 0.021</td>
<td>0.962 ± 0.039</td>
<td>0.820–1.000</td>
<td>0.740–0.926</td>
</tr>
<tr>
<td>Breast</td>
<td>Scatter size, slope, quartile-quantile Cy</td>
<td>0.993–0.996</td>
<td>0.992 ± 0.021</td>
<td>0.833 ± 0.047</td>
<td>0.820–1.000</td>
<td>0.625–0.740</td>
</tr>
</tbody>
</table>

**Fig. 1** ROC curves for LNs of the three cancer types. Blue line, colorectal cancer; black line, gastric cancer; green line, breast cancer. The ROC curves indicate superior classification performance for colorectal and gastric cancers compared with breast cancer. ROC = receiver-operator characteristic.
freshly excised LNs. This system allowed LNs to be scanned over their entire volume. The scanning apparatus featured a single-element, spherically focused, ultrasound transducer (PI-30; Olympus NDT, Waltham, MA) with a 12.2-mm focal length and 6.1-mm aperture. The transducer had a center frequency of 25.6 MHz and a $-6$-dB bandwidth that extended from 16.4 to 33.6 MHz. We digitized the received RF echo signals at a 400-MHz sampling frequency with an accuracy of 8 bits. Scan vectors were uniformly spaced by 25 $\mu$m in X and Y directions across the entire scan volume to acquire complete full-volume 3D data from each LN [38,39]. Typical scanning time ranged from 5 to 30 min, depending on the size of the LN.

Fig. 2 — Illustrative QUS images: 3D cross-sectional parametric images displaying effective scatter-size estimates. (A) 3D cross-sectional parametric images of a benign locoregional LN from a colon cancer patient. (B) 3D cross-sectional parametric images of a locoregional LN with diffusely metastatic adenocarcinoma from a different colon cancer patient. Parametric cross-sectional B-mode images are shown with overlaid color-coded effective scatter-size estimates. Bottom right panel of each figure displays the co-registered histology of the bottom left panel. (Color version of figure is available online.)

Fig. 3 — Illustrative QUS images: 3D cross-sectional parametric images displaying effective scatter-size estimates. (A) 3D cross-sectional parametric images of a benign locoregional LN from a gastric cancer patient. (B) 3D cross-sectional parametric images of a locoregional LN with diffusely metastatic adenocarcinoma from a different gastric cancer patient. Parametric cross-sectional B-mode images are shown with overlaid color-coded effective scatter-size estimates. Bottom right panel of each figure displays the co-registered histology of the bottom left panel. (Color version of figure is available online.)
2.4. Histology processing

Immediately after ultrasound data acquisition, we inked individual dissected LNs to retain orientation for subsequent reconstruction of node histology in 3D and 3D correlations with QUS results. We bisected inked nodes and then fixed them in 10% formalin for at least 6 h, followed by paraffin processing. We then embedded nodes into paraffin block cassettes. We used a step-sectioning procedure and cut 3-μm-thin sections at 50-μm steps from each paraffin block, then stained them with H&E. Two pathologists examined all slides microscopically.

Finally, we obtained fine-resolution (0.23-μm/pixel) digital photomicrographs of the slides using a virtual digital microscopy scanner (NanoZoomer 2.0-HT; Hamamatsu, Hamamatsu City, Japan). We demarcated metastatic regions using Hamamatsu digital editing software. We performed 3D histology reconstruction and compared 3D histology with 3D QUS images to train and evaluate the classifier, and to verify results.

2.5. Quantitative ultrasound parameter estimation

In this blinded study, an investigator at Riverside Research (New York, NY) analyzed the acquired ultrasound data; the investigator was blinded to the histology results obtained at the Kuakini Medical Center in Hawaii. After all analyses were completed, we compared the QUS and histology results. As described previously [38,39], we estimated QUS parameters based on spectrum analysis and envelope statistics from the acquired RF echo-signal data. These QUS methods are only briefly summarized here.

After image segmentation to separate saline and perinodal fibroadipose tissue from the nodal region, we analyzed acquired RF echo-signal data using a series of overlapping 3D cylindrical regions of interest (ROIs) that were 1 mm long and 1 mm in diameter. We computed an average power spectrum normalized to a water-oil interface from the echo signals in the ROI to obtain four spectrum-analysis–based QUS estimates. A straight-line scattering model provided the spectral slope and spectral intercept [38]. A spherical Gaussian
scattering model provided the effective scatter size and acoustic concentration [38].

We computed the envelopes of the RF signals within each ROI; analyses of probability-density functions of the envelope signals provided the four additional QUS estimates. Analyses included application of Nakagami and Homodyned-K statistics models to the envelope signals to derive Nakagami $\alpha$ and Nakagami $\mu$ from the Nakagami distribution, and Homodyned-K $m$ and Homodyned-K $k$ from the Homodyned-K distribution [39]. Finally, we obtained the remaining five QUS estimates using a modified quantile-quantile plot. These estimates were the coordinates of the intersection of low-amplitude and high-amplitude regressions ($C_x$ and $C_y$) and three slopes estimates ($S_l$, $S_h$, and $S_a$), and were obtained by fitting two regression curves to the modified quantile-quantile plot. These five quantile-quantile estimates quantified the difference between the probability-density functions of the ROI and the Rayleigh-distribution probability-density functions [40].

### 2.6. Classification

We used all QUS estimates and histologic examination results to classify cancerous and noncancerous LNs using linear-discriminant analysis. Linear-discriminant analysis combined the 13 different QUS estimates to maximize the differentiation between benign and metastatic tissue in cancer-free and cancer-filled LNs using 50-µm step-sectioning histology as the reference standard. In addition, we implemented a stepwise approach to remove QUS estimates from linear-discriminant analysis when they did not significantly contribute to classification performance.

Histologic differences between LNs of colorectal and gastric cancer patients compared with LNs of breast cancer patients affect the associated QUS estimates for each type of LN metastasis. Consequently, we obtained distinct classifiers for LNs of colorectal and gastric versus breast cancer, rather than across the entire sample population. Classifier quality was expressed as the area under a receiver-operator characteristics (ROCs) curve ($A_z$). The $A_z$ values provided quantitative comparisons of classifier performance for different combinations of QUS estimates.

We developed an interactive graphical user interface (GUI) to permit virtual 3D dissection and exploration of freshly dissected LNs; the GUI displays linked, orthogonal, mouse-selected, cross-sectional views of the node with a histology plane that matches the XY ultrasound plane. The interactive display consisted of a grayscale B-mode plane of the 3D volume with overlaid color-encoded QUS estimate or cancer probability values. We estimated cancer probabilities using a Bayesian approach based on the discriminant score, which we described in detail in our previous study [41].
3. Results

3.1. Classification performance

The Table shows Az values for classification of 290 LNs from 160 patients based on linear-discriminant analysis of the QUS-estimate values. The table also indicates the type of primary cancer and the QUS estimates used as classifiers for each Az value.

Figure 1 displays the ROC curves for LNs of the three cancer types. The ROC curves made the superior classification performance for colorectal and gastric cancers compared with breast cancer readily apparent.

Of 146 LNs of colorectal cancer patients, 23 were metastatic. As shown in Figure 1, linear-discriminant analysis gave an Az of 0.952 ± 0.021 (95% confidence interval [CI]: 0.911–0.993) and sensitivity of 91.3% (corresponding specificity, 87.0%). Of 26 LNs of gastric cancer patients, five were metastatic; linear-discriminant analysis gave an Az of 0.962 ± 0.039 (95% CI: 0.807–1.000). Of 118 LNs of breast cancer patients, 17 were metastatic; linear-discriminant analysis gave an Az of 0.833 ± 0.047 (95% CI: 0.741–0.926) and sensitivity of 88.2% (corresponding specificity, 62.5%). As indicated by the Az values, excellent classification was achieved for LNs of colorectal cancer and gastric cancer patients. The total number of LNs analyzed for gastric cancer is less than the number of LNs analyzed for colorectal cancer and breast cancer. The classification performance of LNs of colorectal cancer patients was superior to the classification achieved for axillary LNs of breast cancer patients; however, the breast cancer classification results were still satisfactory.

3.2. Illustrative QUS images

Figures 2 and 3 show examples of QUS information expressed as 3D images of QUS-estimate values. These figures respectively illustrate QUS-estimate images of representative benign LNs and diffusely metastatic LNs of colorectal and gastric cancer patients. Segmentation results are color-encoded in green and red. The figures show parametric cross-sectional images displaying effective scatter-size estimates in three orthogonal planes within the 3D volume. The H&E-stained histology shown in the lower right corresponds to the scatter-size image plane shown in the lower left.

Average effective scatter-size estimates were 22.96 μm for the benign LN shown in Figure 2A and 33.36 μm for the metastatic LN in Figure 2B. Comparison of the two bottom panels of Figure 2A and 2B shows that these illustrative QUS
images suggest that larger effective scatter size may reliably indicate metastases in LNs of colon cancer patients. Average effective scatter-size estimates were 28.69 mm for the benign LN shown in Figure 3A and 36.69 mm for the metastatic LN in Figure 3B. Comparison of the two bottom panels of Figure 3A and 3B shows that these illustrative QUS images suggest that larger scatter size may reliably indicate metastases in LNs of gastric cancer patients.

For LNs of colorectal and gastric cancers, metastatic LNs displayed larger scatter-size values than cancer-free LNs. These illustrative results suggest that larger scatter size may reliably indicate metastases in LNs of patients with colorectal cancer and gastric cancer. This shows how even a single QUS estimate alone, scatter-size, could aid in identifying suspicious regions.

3.3. 3D interactive GUI with cancer probability images and depiction of micrometastases

A custom GUI displayed 3D QUS and matching 3D histology images for virtual LN interactive evaluation. Figures 4 and 6 show screen captures from this GUI for a partially metastatic LN from a colorectal cancer patient and an LN from a breast cancer patient, respectively. The GUI displays three conventional B-mode ultrasound images from orthogonal planes X, Y, and Z augmented with overlaid color-coded cancer probability images. The lower right image displays the co-registered XY-plane histology with green outlining cancerous regions indicated in Figures 4 and 6. Comparisons of the XY-plane QUS cancer probability B-mode image with the histology image shows an excellent match between the QUS-based depiction of cancerous regions and the histologically determined micrometastatic and macrometastatic foci. In contrast to Figures 4 and 6, Figures 5 and 7 illustrate how the region classified by QUS-based depiction of cancer probability of <25% matches the histologically proven benign regions.

4. Discussion

4.1. Evolution of metastases detection in LNs using HF-QUS methods

Conventional, clinical, B-mode ultrasound images (<15 MHz) are qualitative and operator and system dependent. Because QUS processing exploits information present in the RF echo signals that is discarded by conventional ultrasound image
processing, QUS methods are sensitive to the microstructural features of tissue that cannot be assessed using conventional imaging methods. The theoretical framework for QUS originally was developed in the 1980s [42]. Since then, QUS approaches for tissue characterization have been extended and refined [38,39,43–58]. In this study, we used HF-QUS (>15 MHz) to ensure sensitivity to small features of tissue micro-architecture on the scale of tens of micrometers. Despite limitations in penetration depth imposed on HF-QUS by frequency-dependent attenuation, the small sizes of the great majority of clinically encountered LNs make HF-QUS applicable for guiding pathologists to suspicious regions in dissected LNs. Furthermore, in this study, we carefully removed excess perinodal adipose tissue during the lymph node retrieval procedure, leaving 0.3–0.5 mm of the surrounding fat layer. In addition to minimizing the attenuation issue, this approach ensured that the entire nodal volume was adequately sampled for entire-volume histology processing. Although we removed the excess perinodal fat layer for this study, we believe that we can better address attenuation concerns once a dedicated system is developed (e.g., by optimizing transmitted power and frequency to increase the penetration depth). In an optimized system, the proposed QUS methods may be potentially applicable to freshly excised surgical specimens, such as colectomy specimens and breast axillary lymph node dissection specimens, before the LN harvest performed by pathologists.

During the early stages of our present study, our group described the basis for 3D HF-QUS methods of LN tissue characterization [38]. Previous studies using linear-discriminant analysis demonstrated that just two of the 13 QUS estimates, effective scatter size and the k parameter using the Homodyned-K distribution, were sufficient to reliably distinguish cancerous from cancer-free LNs of patients with colorectal cancer and gastric cancer. By using these two QUS classifiers alone, 95.0% sensitivity was achieved with 95.7% specificity [39].

Our latest results suggest that HF-QUS methods can reliably identify regions of LNs that are suspicious for LN metastases of all three cancer types investigated. Identification of suspicious LNs was successful not only for diffusely metastatic LNs, but also for LNs with micrometastases.

In our previous studies, all colorectal and gastric cancer patients enrolled had adenocarcinomas. LNs of both colorectal and gastric cancer patients were analyzed together because of the histologic similarity between these types of LNs and the small number of enrolled gastric cancer patients [39]. Metastatic colorectal cancer and gastric cancer in LNs had larger QUS effective scatter size compared with benign LNs. In general, tumor cells are larger than lymphocytes. This may explain the larger QUS estimate of effective scatter size observed in metastatic LNs of colorectal and gastric cancer patients compared with benign LNs. The LN metastases of other cancers are known to have different microscale morphology; for example, LNs of breast cancer patients often present with fatty ingrowths. The variability of axillary LN morphology is well known, and attenuation through the fatty ingrowth in axillary LNs of breast cancer patients, compared with LNs of colorectal cancer patients, may degrade QUS-based classification. This suggests that different QUS estimates combinations may be more effective for detecting regions suspicious for metastases for different types of primary tumors.

4.2. Interactive 3D cancer probability images as a future pathology tool

Interactive 3D cancer probability images based on HF ultrasound can be made into a small, low-cost pathology tool that can scan LNs immediately after the surgical specimen is received in the pathology laboratory. In this study, we used a custom research scanning system. The scanning time varied between 5 and 30 min, depending on the size of the LN. However, once this method is incorporated into a dedicated system with much faster motors, we believe that the scanning time can be shortened to <2 min/LN for an entire-volume 3D nodal examination.

This will provide a fast, reliable, and operator-independent technique that can scan fresh LNs and provide interactive, real-time, B-mode, ultrasound images with color-encoded cancer probability overlays, as shown in Figures 4, 5, 6 and 7. The LNs also can be scanned intraoperatively immediately after lymphadenectomy or excision of the surgical specimen while the specimen remains intact. This may benefit cancer management by aiding decisions that depend on LN status (e.g., on the number of total metastatic LNs). This tool may assist in detecting small metastatic foci that would be missed by standard, intraoperative, touch-prep or frozen-section procedures, which is especially important for breast cancer sentinel LN biopsy. If QUS-based cancer probability images show regions that are highly suspicious for metastases (e.g., regions with a cancer probability of >75%), the pathologist can target the intraoperative touch-prep procedure or frozen-section procedure to those highly suspicious regions. Also, the operator would be able to adjust the sensitivity and specificity to establish a preferred threshold for decision choices (e.g., to obtain 100% sensitivity with the corresponding specificity). The first potential use for this novel tool would be to guide pathologists to suspicious regions of LNs for definitive histology; if successful, it potentially can dramatically improve detection sensitivity to small metastatic foci that would be missed using conventional histology methods.

This study was limited by the relatively low enrollment of gastric cancer patients, compared with colorectal cancer patients. Future enrollment of additional gastric cancer patients may confirm results obtained to date with LNs of colorectal cancer patients. The total number of LNs acquired per enrolled cancer patient also limited the study. We selected only freshly excised LNs, which excluded LNs harvested after formalin fixation or exposure to fat-dissolving solutions. To avoid delay in diagnosis, which may interfere with the standard of care, we limited the number of LNs processed using our full-volume step-sectioning. As a prospective study, we precluded selection bias by sequentially enrolling patients, randomly selecting LNs for the study from the full surgical specimen, and blinding the investigator who selected the LNs from the specimen to clinical information.

In addition to continuing data acquisition and improving the QUS methods, additional studies are being planned to apply these QUS methods to lower ultrasound frequencies, to
effective treatment. all micrometastases is essential for accurate staging and significant metastases is of great concern because detection of micrometastases that are missed by conventional single-reliably detect metastases in LNs. Furthermore, these tech-
ing the permanent histology section to the suspicious region. thus more accurate tumor-node-metastases staging by target-
may contribute to more sensitive detection of metastases, and prognosis in all three cancer types. This future pathology tool
metastases changes the node status of the tumor-node-
cancer types in the pathology lab. The number of regional LN
will enable pathologists to identify suspicious LNs of all three
lenges at higher frequencies, and will also be intended to scan nonsentinel axillary LNs of breast cancer patients. This may
resolving the current controversy over sentinel LN biopsy, and consequently, may contribute to improving surgical treatment and management of breast cancer.

The ex vivo application with higher ultrasound frequencies will enable pathologists to identify suspicious LNs of all three cancer types in the pathology lab. The number of regional LN metastases changes the node status of the tumor-node-
prognosis in all three cancer types. This future pathology tool
may contribute to more sensitive detection of metastases, and thus more accurate tumor-node-metastases staging by target-
ing the permanent histology section to the suspicious region.

Our results suggest that the described 3D QUS methods can reliably detect metastases in LNs. Furthermore, these tech-
iques may enable detection of the clinically relevant fraction of micrometastases that are missed by conventional single-
section histology. The high probability of missed clinically
significant metastases is of great concern because detection of all micrometastases is essential for accurate staging and
effective treatment.

Acknowledgments

The authors thank Gregory K. Kobayashi, MD, FCAP, Clifford C. Wong, MD, FCAP, Patricia Kim, MD, FCAP, and Conway Fung, MT, at the Department of Pathology, Kuakini Medical Center, Honolulu, Hawaii, for pathology and histology expertise. Emi Saegusa-Beecroft thanks Professor Keisho Marumo, MD, PhD, Department of Orthopedic Surgery, Jikei University School of Medicine, Tokyo, Japan, for his mentorship. Research reported in this publication was supported by the National Institutes of Health under grant CA 100183, awarded to Ernest J. Feleppa, PhD. The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health.

REFERENCES


Oncol 2005;23:7703.


